Monitoring cardiac function in intensive care

S M Tibby, I A Murdoch

Systolic cardiac function results from the interaction of four interdependent factors: heart rate, preload, contractility, and afterload. Heart rate can be quantified easily at the bedside, while preload estimation has traditionally relied on invasive pressure measurements, both central venous and pulmonary artery wedge. These have significant clinical limitations; however, adult literature has highlighted the superiority of several novel preload measures. Measurement of contractility and afterload is difficult; thus in clinical practice the bedside assessment of cardiac function is represented by cardiac output. A variety of techniques are now available for cardiac output measurement in the paediatric patient. This review summarises cardiac function and cardiac output measurement in terms of methodology, interpretation, and their contribution to the concepts of oxygen delivery and consumption in the critically ill child.

A ccurate assessment and monitoring of cardiac function in the intensive care unit (ICU) is essential, as the heart is one of the commonest organs to fail during critical illness.\(^1\) In addition, other failing organs as well as therapies supporting these organs may have an indirect effect on myocardial performance.\(^2\) The need to monitor cardiac function is underlined by the fact that a low flow state carries a higher mortality in certain diseases.\(^3\) As flow cannot be consistently estimated clinically, we often titrate therapies to maintain an acceptable blood pressure. While maintenance of an adequate perfusion pressure to organs is vital, it can be seen from table 1 and equation 1 that blood pressure is affected by cardiac output (CO) and systemic vascular resistance (SVR).

\[
\text{Mean blood pressure} = \text{cardiac output} \times \text{systemic vascular resistance} \quad (1)
\]

Thus a low blood pressure may be secondary to a low CO, low SVR, or both. Conversely a normal blood pressure can exist in the face of decreased CO if SVR is high. A low CO may occur for many reasons including inadequate vascular volume, excessive afterload, poor contractility, myocardial restriction, diastolic dysfunction, valvular stenosis/insufficiency, or an arrhythmia. Any of these abnormalities may coexist, and can fluctuate during the course of an illness, meaning that an appropriate therapy at one point in time can become inappropriate as the patient’s clinical state alters.\(^4\) Thus the role of cardiac monitoring encompasses assessment of the initial haemodynamic state, judging response to therapy, and ongoing evaluation of change in haemodynamic state with disease progression.

In this review we will discuss various aspects affecting cardiac function and its closely related parameter CO, outline modalities for CO measurement, examine some of the qualitative parameters pertaining to the adequacy of CO, and finally attempt to integrate these parameters into the wider spectrum of monitoring metabolic “wellbeing” in the critically ill child, with particular reference to the oxygen delivery/consumption balance.

WHAT IS CARDIAC FUNCTION?

Cardiac systolic function is the net product of four interrelated variables: heart rate, preload, contractility, and afterload.\(^5\) Quantification of these individual components of cardiac function in the clinical setting poses two major problems. First, the methods used require either invasive (usually ventricular) pressure and volume measurements, or highly specialised echocardiographic techniques. The invasive methods usually entail manipulation of one of the elements while measuring another (for example, altering preload to calculate contractility from either end systolic elastance or preload recruitable stroke work\(^6\)), which is impractical in the critically ill patient. Second, all components display a degree of interdependence, thus an apparent deficiency in one element of cardiac function may actually be secondary to a problem with one or more of the other facets. A simple example involves a tachyarrhythmia (heart rate) reducing the time for diastolic ventricular filling (preload). Here preload restoration involves treating the arrhythmia, rather than volume replacement.

Early work aimed at quantifying myocardial performance centred on systolic function, however it is now known that diastolic mechanics are also crucial.\(^7\) Diastolic function encompasses both the rate and degree of ventricular relaxation, containing active and passive components.\(^8\) Like systolic performance, this parameter is not easily interpreted at the bedside.\(^9\)\(^10\)

The interplay of heart rate, preload, contractility, and afterload results in CO, which is defined as the volume of blood ejected by the heart per minute. As such, CO represents the clinical manifestation of cardiac function, which can be measured at the bedside. In children CO is often

**Abbreviations:** CO, cardiac output; ICU, intensive care unit; SVR, systemic vascular resistance
CHOICE OF TECHNIQUE FOR CO MONITORING

Shephard et al have identified eight desirable characteristics for any monitoring technique: accuracy, reproducibility, rapid response time, operator independence, ease of application, no morbidity, continuous use, and cost effectiveness. Unfortunately, no such technique exists for CO measurement in either paediatric or adult practice; thus the choice of method may vary depending on the patient and the clinical situation. A detailed description of all techniques available for CO measurement is beyond the scope of this article and is available elsewhere. Instead we will broadly outline the measurement principles below, while specific techniques are summarised in Table 2.

The main principles of CO measurement include the Fick principle, indicator dilution, Doppler ultrasound, bioimpedance, and arterial pulse contour analysis.

The Fick principle

The Fick principle for flow measurement is now over a century old, and relates CO to oxygen consumption and the arteriovenous oxygen content difference (table 1). The equation may also be modified using CO2 production and content, which has been adapted to provide non-invasive estimation. Traditional techniques for measuring oxygen consumption, namely the Douglas bag, spirometry, and more recently mass spectrometry, have limited the clinical utility of this technique in the ICU. However, with the advent of portable metabolic monitors adapted for paediatric use, this technique is now possible in children and infants.

Dilution techniques

Dilution techniques have existed for many years. Briefly, blood flow can be calculated following a central venous injection of an indicator by measuring the change in indicator concentration over time at a point downstream of the injection, provided that a series of conditions are met. These include complete mixing of the indicator and blood, no loss of indicator between injection and measurement, no anatomical shunt, and minimal valve regurgitation. The earliest indicator used was dye, and later temperature with the introduction of the pulmonary artery catheter in the early 1970s, followed by transpulmonary thermodilution in the 1990s. A new indicator, lithium chloride, has recently been described in adults and children.

Doppler ultrasound

Cardiac output may be calculated using Doppler ultrasound in conjunction with 2D echocardiography. Blood velocity is calculated from the frequency shift of reflected ultrasound waves using the Doppler principle. This is usually measured in the aorta, from either the transthoracic or transoesophageal
Table 2  Methods of paediatric cardiac output measurement

<table>
<thead>
<tr>
<th>Variables measured in addition to cardiac output</th>
<th>Principle</th>
<th>Method</th>
<th>Advantages</th>
<th>Disadvantages</th>
</tr>
</thead>
<tbody>
<tr>
<td>Oxygen consumption</td>
<td>Direct Fick</td>
<td>Indirect calorimetry</td>
<td>Accurate if applied correctly26 77 Requires a site for mixed venous blood sampling, inaccurate with endotracheal tube leak, pneumothorax, or FIO 2 &gt;0.5 (unless mass spectrometry used)78</td>
<td></td>
</tr>
<tr>
<td>Dilution</td>
<td>Thermodilution:</td>
<td>Proven track record</td>
<td>Semicontinuous mode available79</td>
<td>Inaccurate at low flows, low but significant morbidity: infection, bleeding, catheter knotting81</td>
</tr>
<tr>
<td>Pulmonary artery</td>
<td>Easy access in small patients, repeatable</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Thermodilution: Transpulmonary dye</td>
<td>Accurate</td>
<td>Sequential measurements limited by dye clearance, commercial availability of dye and devices31, utilises pre-existing central venous and arterial lines</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Thermodilution: Lithium chloride</td>
<td>Accurate</td>
<td></td>
<td>Theoretical risk of toxicity, requires blood sample with each measurement and arterial lines</td>
<td></td>
</tr>
<tr>
<td>Doppler ultrasound</td>
<td>Supplies structural and functional information</td>
<td></td>
<td>Inter- and intra-user variability83 84</td>
<td></td>
</tr>
<tr>
<td>Transoesophageal Doppler</td>
<td>Continuous, minimal user training, repeatable, accurate</td>
<td></td>
<td>High accuracy, low risk, critical line insertion is difficult, which may interfere with signal quality</td>
<td></td>
</tr>
<tr>
<td>Bioimpedance</td>
<td>Non-invasive</td>
<td></td>
<td>Doubtful accuracy in critical illness85</td>
<td></td>
</tr>
<tr>
<td>Intracardiac</td>
<td>ACCURATE</td>
<td>Highly invasive</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Arterial pulse contour analysis</td>
<td>Continuous</td>
<td></td>
<td></td>
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</tbody>
</table>

**Bioimpedance**

Thoracic bioimpedance involves the placement of voltage sensing and current transmitting electrodes on the chest, which may be regarded as a conductor whose impedance is altered by changes in blood volume and velocity with each heartbeat. Stroke volume is calculated from an equation involving baseline and maximum rate of change in impedance, ventricular ejection time, and thoracic segment length. The accuracy of this technique is dramatically increased (along with its invasiveness) when the conductance catheter is placed directly in the left ventricle, rather than on the chest wall.

**Arterial pulse contour analysis**

Erlanger suggested a relation between CO and arterial pulse contour nearly a century ago. This led to the development of a number of analytical methods quantifying change in stroke volume based on characteristics of the arterial pulse pressure wave. The advent of fast computer microprocessors has meant that several of these methods are now commercially available, providing stroke volume and CO on a continuous basis. However, all must be calibrated using another method of CO measurement.

**INTERPRETATION OF CO**

As discussed earlier, it is imperative that the clinician has a thorough understanding of the limitations, accuracy, and risks of the method used to determine CO, to avoid generation of spurious data. Perhaps the greater challenge however lies in “understanding the number” once it is generated. We suggest that CO should ideally be interpreted from four aspects:

1. A quantitative element
2. A qualitative element
3. A temporal element
4. As part of a global (an ideally a regional) assessment of metabolic wellbeing.

Points 1–3 can be summarised as: the CO is “x” l/min, which is adequate/inadequate for this patient at this time. Integration of CO into a global metabolic assessment necessitates an appreciation of the contribution of CO to oxygen delivery, and an understanding of the balance between oxygen delivery and consumption (table 1, fig 1). From a clinical perspective, this requires the consideration of four questions:

1. Is the delivery of oxygen adequate to meet the metabolic need of the patient, both on a global and a regional scale?
2. Is oxygen delivery occurring with an adequate perfusion pressure?
(3) Is the patient able to utilise the oxygen delivered?

(4) If the answer to any of the above is “no”, why is this so?

**ADEQUACY OF CO AND OXYGEN DELIVERY**

A variety of clinical, laboratory, and physiological variables exist which may help to indicate adequacy of CO and/or oxygen delivery.

**Global indicators**

Lactate

With the advent of automated blood lactate analysers, interest in this parameter has seen an explosion in the last decade. Simplistically, an increased blood lactate is thought to represent anaerobic metabolism, which occurs when oxygen delivery is inadequate, or oxygen utilisation is impaired (tissue dysoxia). Recent evidence suggests that this may be an oversimplification, as other factors such as increased glycolytic flux and lactate clearance may also play a part. Nonetheless this parameter has prognostic value, particularly when followed temporally, thus any increase in blood lactate is a cause for concern and the aetiology must be aggressively sought.

Mixed venous oxygen saturation

From the Fick principle (table 1) it can be seen that a low CO or excessive oxygen consumption can be partially compensated by an increase in the arteriovenous oxygen difference. This commonly translates into a fall in mixed venous saturation, as arterial blood is often almost fully saturated and the contribution of dissolved oxygen to total oxygen content is usually minimal. This is an early compensatory mechanism, and may precede a rise in blood lactate. Again, from the Fick equation, it can be seen that, at a constant oxygen consumption and arterial oxygen saturation, the relation between change in mixed venous saturation and CO is not linear, in other words a given decrease in mixed venous saturation may represent a comparatively larger decrease in CO (fig 2).

**Figure 1**  Factors affecting oxygen delivery and consumption. BP, systemic blood pressure; SVR, systemic vascular resistance; VO2, oxygen consumption; A-V, atrioventricular; LVES, left ventricular end systolic. *Common intensive care scenarios augmenting intrathoracic pressure include mechanical ventilation, pneumothorax, pleural/pericardial fluid collections.

**Figure 2**  Relative change in cardiac index versus change in mixed venous oxygen saturation. The relation assumes the following to be constant: oxygen consumption 180 ml/min/m², haemoglobin concentration 120 g/l, arterial oxygen saturation 98%. Baseline cardiac index is 4 l/min/m².

Mixed venous blood should ideally be taken from the pulmonary artery or the right ventricle; however, these sites may be inaccessible in the small infant. Right atrial catheters may, in theory selectively sample desaturated coronary venous blood; however, in practice this does not seem to be the case. Central venous sites have been advocated, although this is subject to ongoing debate. The oxygen saturation of central venous blood from either the superior or inferior vena cavae...
will not be identical to true mixed venous blood, because of age and disease related variations in flow and oxygen consumption between the upper and lower body. However the differences may not be great, and may be suitable for trend following. Venous oxygen saturation will also be partly dependent on arterial oxygen saturation, thus the arterio-venous difference or the oxygen extraction ratio are better alternatives in the face of lung pathology (table 1). The inverse of the oxygen extraction ratio is known as the oxygen excess factor, or \( \Omega \). Omega represents the ratio of oxygen delivery to consumption, and has an advantage over CO in that it may be calculated in the setting of an anatomical shunt. 

**Regional indicators**

An apparently adequate global oxygen delivery may mask significant regional abnormalities. Unfortunately, comprehensive clinical tools assessing all aspects of regional perfusion are lacking; however, several of the common methods are detailed below.

**Capillary refill and core-peripheral temperature difference**

Provided that it is measured correctly, capillary refill has proven useful as a marker of hypovolaemia and perhaps poor myocardial function during acute assessment and early resuscitation. The significance of this parameter in ICU is less clear, and may be obscured by confounding factors such as fever, ambient temperature, and vasoactive medication use. In the ICU there is a surprising positive correlation with central venous pressure \( (r = 0.34) \), which is perhaps as much of a commentary on the limitation of central venous pressure as a marker of hypovolaemia. Capillary refill correlates negatively \( (r = -0.46) \) with stroke volume, and the optimal predictive value for a reduced stroke volume comes from a refill time \( \geq 6 \) seconds. There is no correlation with systemic vascular resistance. Despite these limitations, we believe capillary refill has a useful role in temporal haemodynamic monitoring. It is a quick, easy bedside test, and a dramatic change in this parameter should alert the clinician to a more detailed haemodynamic assessment of the patient. The correlation between core-peripheral temperature difference and invasive haemodynamic parameters is very poor; this parameter offers no real advantage over capillary refill.

**Other regional indicators**

A change in the level of consciousness in a patient with septic shock may be erroneously interpreted as secondary to “meningitis” or cerebral oedema; in reality this often represents cerebral hypoxia caused by lack of blood flow, and is, in our experience an ominous sign. Splanchnic oxygen delivery has been quantified using gastric tonometry. Here a semipermeable balloon is placed in the stomach, and gastric mucosal \( CO_2 \) is allowed to equilibrate with the medium in the balloon. The medium may be either saline or recirculating gas, the latter method being the more accurate; Regional hyperfusion or failure of oxygen utilisation are revealed by a large difference between mucosal \( PCO_2 \), and arterial blood \( PCO_2 \). Illness may be a clinical manifestation of splanchnic hyperfusion; however, other causes must always be excluded. Similarly, one of the causes of acute derangement of liver transaminases may be inadequate hepatic oxygen delivery, and lack of renal blood flow may result in poor urine output and a rise in the serum urea and creatinine.

**PERFUSION PRESSURE**

Global perfusion pressure is measured via invasive arterial blood pressure monitoring. However, without CO measurement two erroneous inferences are possible: first, that an “adequate” blood pressure signifies an “adequate” \( CO \); and second that manoeuvres that raise the blood pressure also result in elevation of \( CO \) (equation 1). In fact neither may be the case. The failing myocardium responds poorly to a high systemic vascular resistance; thus an increase in blood pressure may result in a fall in \( CO \); conversely lowering the systemic vascular resistance with vasodilator therapy may produce a considerable gain in terms of \( CO \) despite a small drop in blood pressure.

**OXYGEN CONSUMPTION**

Oxygen consumption can now be measured at the bedside, even in the smallest patients, the commonest ICU method being indirect calorimetry. Providing that oxygen delivery and perfusion pressure are adequate, an inability to consume oxygen may be inferred without direct measurement from the combination of a raised blood lactate with a high mixed venous oxygen saturation.

**IDENTIFYING THE SOURCE OF INADEQUATE OXYGEN DELIVERY OR EXCESSIVE CONSUMPTION**

**Oxygen delivery**

Two of the components of oxygen delivery, haemoglobin concentration and arterial haemoglobin oxygen saturation, can be easily determined (table 1). The cause of a deficiency in the third component, \( CO \) is not always apparent, as this can be caused by abnormalities in heart rate, preload, contractility, afterload, or any combination of the four.

**Heart rate**

Heart rate is the easiest parameter to measure at the bedside. Cardiac output can be adversely affected by extreme sinus tachycardia (for example, with hypovolaemia or excessive inotrope use), bradycardia, or any arrhythmia producing loss of atrioventricular synchrony.

**Preload**

Preload encompasses the variety of factors resulting in ventricular end diastolic volume. It is important to appreciate that the preload of the right and left heart are not necessarily the same. The two commonly used measures of preload, namely central venous pressure (right heart) and pulmonary artery occlusion pressure (left heart) both have clinical limitations. This is because many factors affect the ability of a pressure measurement to act as a marker of volume status, including venous capacitance, cardiac chamber compliance, valve competence, pulmonary artery pressures, and the ability of the lung to function as a Starling resistor with positive pressure ventilation, to name a few. However it is probably reasonable to assume that a low central venous pressure may represent underfilling, and this parameter may be useful for trending.

Two new volume based measures, intrathoracic blood volume and right ventricular end diastolic volume, have been evaluated favourably as preload indicators. Both are calculated from modifications of a thermodilution technique; however, neither has been adequately evaluated in children. Analysis of variation in arterial pulse pressure waveform shows great promise, and can easily be incorporated into routine invasive blood pressure monitoring on a continuous basis. Several transoesophageal Doppler derived parameters have been explored; one has been used successfully in adults to guide intraoperative volume replacement. Two echocardiographic indicators of preload have been suggested. The functional preload index requires specialised software and a series of calculations, thus limiting its clinical use, while interpretation of mitral inflow velocity profiles is often beset by confounding variables. Diastolic dysfunction also affects preload, although controversy exists regarding the interpretation of echocardiographic parameters of diastolic function in certain clinical scenarios.
Contrastility
An adequate bedside measure of contractility does not exist. The echocardiographic stress velocity index has provided insight into pathophysiology, but requires the same technical specifications as the functional preload index. Recently one of the assumptions on which this parameter is based, namely the linear relation between stress velocity (contractility) and end systolic wall stress (afterload) has been questioned, suggesting a reappraisal of its clinical interpretation. Stoke work index represents the area enclosed by the ventricular pressure-volume loop; however, this may be estimated at the bedside from stroke index and arterial pressure measurements (table 1). Although not a true measure of contractility, it allows some insight into cardiac reserve, namely how stoke index (volume) is adjusted in the face of changing afterload.

Afterload
Afterload is defined as the force opposing left ventricular fibre shortening during ventricular ejection in other words left ventricular wall stress. Wall stress can be measured at various shortening during ventricular ejection, in other words left

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