Monitoring cardiac function in intensive care

S M Tibby, I A Murdoch

Systolic cardiac function results from the interaction of four interdependent factors: heart rate, preload, contractility, and afterload. Heart rate can be quantified easily at the bedside, while preload estimation has traditionally relied on invasive pressure measurements, both central venous and pulmonary artery wedge. These have significant clinical limitations; however, adult literature has highlighted the superiority of several novel preload measures. Measurement of contractility and afterload is difficult; thus in clinical practice the bedside assessment of cardiac function is represented by cardiac output. A variety of techniques are now available for cardiac output measurement in the paediatric patient. This review summarises cardiac function and cardiac output measurement in terms of methodology, interpretation, and their contribution to the concepts of oxygen delivery and consumption in the critically ill child.

A ccurate assessment and monitoring of cardiac function in the intensive care unit (ICU) is essential, as the heart is one of the commonest organs to fail during critical illness. In addition, other failing organs as well as therapies supporting these organs may have an indirect effect on myocardial performance. The need to monitor cardiac function is underlined by the fact that a low flow state carries a higher mortality in certain diseases. As flow cannot be consistently estimated clinically, we often titrate therapies to maintain an acceptable blood pressure. While maintenance of an adequate perfusion pressure to organs is vital, it can be seen from table 1 and equation 1 that blood pressure is affected by cardiac output (CO) and systemic vascular resistance (SVR).

\[
\text{Mean blood pressure} = \text{cardiac output} \times \text{systemic vascular resistance} \quad (1)
\]

Thus a low blood pressure may be secondary to a low CO, low SVR, or both. Conversely a normal blood pressure can exist in the face of decreased CO if SVR is high. A low CO may occur for many reasons including inadequate vascular volume, excessive afterload, poor contractility, myocardial restriction, diastolic dysfunction, valvular stenosis/insufficiency, or an arrhythmia. Any of these abnormalities may coexist, and can fluctuate during the course of an illness, meaning that an appropriate therapy at one point in time can become inappropriate as the patient’s clinical state alters. Thus the role of cardiac monitoring encompasses assessment of the initial haemodynamic state, judging response to therapy, and ongoing evaluation of change in haemodynamic state with disease progression.

In this review we will discuss various aspects affecting cardiac function and its closely related parameter CO, outline modalities for CO measurement, examine some of the qualitative parameters pertaining to the adequacy of CO, and finally attempt to integrate these parameters into the wider spectrum of monitoring metabolic “wellbeing” in the critically ill child, with particular reference to the oxygen delivery/consumption balance.

WHAT IS CARDIAC FUNCTION?

Cardiac systolic function is the net product of four interrelated variables: heart rate, preload, contractility, and afterload. Quantification of these individual components of cardiac function in the clinical setting poses two major problems. First, the methods used require either invasive (usually ventricular) pressure and volume measurements, or highly specialised echocardiographic techniques. The invasive methods usually entail manipulation of one of the elements while measuring another (for example, altering preload to calculate contractility from either end systolic elastance or preload recruitable stroke work), which is impractical in the critically ill patient. Second, all components display a degree of interdependence, thus an apparent deficiency in one element of cardiac function may actually be secondary to a problem with one or more of the other facets. A simple example involves a tachyarrhythmia (heart rate) reducing the time for diastolic ventricular filling (preload). Here preload restoration involves treating the arrhythmia, rather than volume replacement.

Early work aimed at quantifying myocardial performance centred on systolic function, however it is now known that diastolic mechanics are also crucial. Diastolic function encompasses both the rate and degree of ventricular relaxation, containing active and passive components. Like systolic performance, this parameter is not easily interpreted at the bedside.

The interplay of heart rate, preload, contractility, and afterload results in CO, which is defined as the volume of blood ejected by the heart per minute. As such, CO represents the clinical manifestation of cardiac function, which can be measured at the bedside. In children CO is often

Abbreviations: CO, cardiac output; ICU, intensive care unit; SVR, systemic vascular resistance
indexing to body surface area, known as cardiac index, with the same set of “normal” values applying (3.5–5.5 l/min/m²) regardless of patient age and size. However, it must be appreciated that the term “normal” may be misleading (see Interpretation of CO below); for example, a low CO is not uncommon following cardiac surgery and may not hold the same poor prognosis as when found in the setting of sepsis.

**WHEN SHOULD CO BE MEASURED?**

Cardiac output measurement is not mandatory for every child admitted to the ICU. The decision to measure CO represents a balance between the risks involved with the measurement process, and the potential benefits gained from the additional haemodynamic information. The latter point requires a thorough understanding of both the modality used and the basic principles of cardiovascular physiology; if both of these criteria are not met there is potential for iatrogenic harm to the patient. For example, a technique with poor repeatability (a high coefficient of variation) may produce two consecutive readings with differing results without a true change in CO. This may falsely be interpreted as a fall in CO, resulting in an unnecessary intervention or therapy. If the clinician understands the modality’s limitations he/she may take the necessary steps to minimise variability (such as measuring during steady state conditions, averaging several consecutive measurements, etc) and is better placed to judge when a difference between two readings represents a true change in CO.

The importance of “understanding the process” of CO measurement has been highlighted in two large studies nearly half of the respondents who could not correctly identify a wedge pressure (a measure of preload, and thus a guide to fluid management), over half could not recognise when the catheter was incorrectly sited in a systemic artery, and many could not quantify the relative influence of individual components of oxygen delivery. However, physicians who scored well tended to have a thorough understanding of both the modality used and the calculation principles below, while specific techniques are summarised in table 2.

**THE FICK PRINCIPLE**

The Fick principle for flow measurement is now over a century old, and relates CO to oxygen consumption and the arteriovenous oxygen content difference (table 1). The equation may also be modified using CO2 production and arteriovenous oxygen content difference. The Fick principle and minimal valve regurgitation. The earliest indicator used between injection and measurement, no anatomical shunt, and minimal valve regurgitation. The earliest indicator used was dye, and later temperature with the introduction of the pulmonary artery catheter in the early 1970s, followed by transpulmonary thermodilution in the 1990s. A new indicator, lithium chloride, has recently been described in adults and children. Briefly, blood flow can be calculated following a central venous injection of an indicator by measuring the change in indicator concentration over time at a point downstream of the injection, provided that a series of conditions are met. These include complete mixing of the indicator and blood, no loss of indicator between injection and measurement, no anatomical shunt, and minimal valve regurgitation. The earliest indicator used was dye, and later temperature with the introduction of the pulmonary artery catheter in the early 1970s, followed by transpulmonary thermodilution in the 1990s. A new indicator, lithium chloride, has recently been described in adults and children.

**Dilution techniques**

Dilution techniques have existed for many years. Briefly, blood flow can be calculated following a central venous injection of an indicator by measuring the change in indicator concentration over time at a point downstream of the injection, provided that a series of conditions are met. These include complete mixing of the indicator and blood, no loss of indicator between injection and measurement, no anatomical shunt, and minimal valve regurgitation. The earliest indicator used was dye, and later temperature with the introduction of the pulmonary artery catheter in the early 1970s, followed by transpulmonary thermodilution in the 1990s. A new indicator, lithium chloride, has recently been described in adults and children.

**Doppler ultrasound**

Cardiac output may be calculated using Doppler ultrasound in conjunction with 2D echocardiography. Blood velocity is calculated from the frequency shift of reflected ultrasound waves using the Doppler principle. This is usually measured in the aorta, from either the transthoracic or transoesophageal

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### Table 1 Common measured and calculated haemodynamic variables

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Formula</th>
<th>Normal range</th>
<th>Units</th>
</tr>
</thead>
<tbody>
<tr>
<td>Cardiac index</td>
<td>CI = CO / body surface area</td>
<td>3.5–5.5 l/min/m²</td>
<td></td>
</tr>
<tr>
<td>Stroke index</td>
<td>SI = CI / heart rate</td>
<td>30–60 ml/min/m²</td>
<td></td>
</tr>
<tr>
<td>Arterial oxygen content</td>
<td>CaO₂ = (1.34 × Hgb × SaO₂) + (PaO₂ × 0.03)</td>
<td>570–670 ml/min/m²</td>
<td></td>
</tr>
<tr>
<td>Oxygen delivery</td>
<td>DO₂ = CI × CaO₂</td>
<td>160–180 (infant VO₂)</td>
<td></td>
</tr>
<tr>
<td>Fick principle</td>
<td>CI = VO₂ / (CaO₂ × CvO₂)</td>
<td>100–130 (child VO₂)</td>
<td></td>
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</tbody>
</table>

| Oxygen extraction ratio    | OER = (SaO₂ – SvO₂) / SaO₂ | 0.24–0.28             |       |
| Oxygen excess factor       | Ω = SaO₂ / (SaO₂ × CvO₂)    | 3.6–4.2               |       |
| Systemic vascular resistance index | SVRI = 79.9 × (MAP – CVP) / CI | 800–1600 dyns/cm²/m² |       |
| Left ventricular stroke work index | LVSWI = SI × MAP × 0.0136 | 50–62 (adult) g-m/m²  |       |

CO, cardiac output; CI, cardiac index; CVP, central venous pressure (mmHg); CaO₂, arterial oxygen content; CvO₂, mixed venous oxygen content; DO₂, oxygen delivery; Hgb, haemoglobin concentration (g/l); LVSWI, left ventricular stroke work index; MAP, mean arterial pressure (mmHg); OER, oxygen extraction ratio; PaO₂, partial pressure of dissolved oxygen; SaO₂, arterial oxygen saturation; SvO₂, mixed venous oxygen saturation; SI, stroke index; SVRI, systemic vascular resistance index; VO₂, oxygen consumption; Ω, oxygen excess factor.

*The equations given for OER and Ω are only valid if the contribution from dissolved oxygen is minimal. If this is not the case, oxygen content (CaO₂, CvO₂) must be substituted for saturation (SaO₂, SvO₂)."
Table 2

<table>
<thead>
<tr>
<th>Principle</th>
<th>Method</th>
<th>Variables measured in addition to cardiac output</th>
</tr>
</thead>
<tbody>
<tr>
<td>Direct Fick</td>
<td>Indirect calorimetry</td>
<td>Oxygen consumption, energy expenditure, total body oxygen consumption</td>
</tr>
<tr>
<td>Thermodilution</td>
<td>Pulmonary artery</td>
<td>Oxygen saturation, oxygen content, oxygen transport</td>
</tr>
<tr>
<td>Transoesophageal Doppler</td>
<td>Frequency analysis</td>
<td>Oxygen saturation, oxygen content, oxygen transport, blood flow</td>
</tr>
<tr>
<td>Modified Windkessel</td>
<td>Bioimpedance</td>
<td>Oxygen saturation, oxygen content, oxygen transport, blood flow</td>
</tr>
</tbody>
</table>

**Methods of paediatric cardiac output measurement**

<table>
<thead>
<tr>
<th>Principle</th>
<th>Method</th>
<th>Advantages</th>
<th>Disadvantages</th>
</tr>
</thead>
<tbody>
<tr>
<td>Direct Fick</td>
<td>Indirect calorimetry</td>
<td>Accurate if applied correctly</td>
<td>Requires a site for mixed venous blood sampling, inaccurate with endotracheal tube leak, pneumothorax, or FIO2 &gt; 0.5 (unless mass spectrometry used)</td>
</tr>
<tr>
<td>Thermodilution</td>
<td>Pulmonary artery</td>
<td>Proven track record</td>
<td>Variations in CO with respiratory cycle, difficult access in small patients, inaccurate at low flows, low but significant morbidity: infection, bleeding, catheter knotting</td>
</tr>
<tr>
<td>Transoesophageal Doppler</td>
<td>Frequency analysis</td>
<td>Accurate</td>
<td>Variations in CO with respiratory cycle, difficult access in small patients, inaccurate at low flows, low but significant morbidity: infection, bleeding, catheter knotting</td>
</tr>
<tr>
<td>Modified Windkessel</td>
<td>Bioimpedance</td>
<td>Accurate</td>
<td>Doubtful accuracy in critical illness</td>
</tr>
</tbody>
</table>

**Bioimpedance**

Thoracic bioimpedance involves the placement of voltage sensing and current transmitting electrodes on the chest, which may be regarded as a conductor whose impedance is altered by changes in blood volume and velocity with each heartbeat. Stroke volume is calculated from an equation involving baseline and maximum rate of change in impedance, ejection time, and thoracic segment length. The accuracy of this technique is dramatically increased (along with its invasiveness) when the conductance catheter is placed directly in the left ventricle, rather than on the chest wall.

**Arterial pulse contour analysis**

Erlanger suggested a relation between CO and arterial pulse contour nearly a century ago. This led to the development of a number of analytical methods quantifying change in stroke volume based on characteristics of the arterial pulse pressure wave. The advent of fast computer microprocessors has meant that several of these methods are now commercially available, providing stroke volume and CO on a continuous basis. However, all must be calibrated using another method of CO measurement.

**INTERPRETATION OF CO**

As discussed earlier, it is imperative that the clinician has a thorough understanding of the limitations, accuracy, and risks of the method used to determine CO, to avoid generation of spurious data. Perhaps the greater challenge however lies in “understanding the number” once it is generated. We suggest that CO should ideally be interpreted from four aspects:

1. A quantitative element
2. A qualitative element
3. A temporal element
4. As part of a global (an ideally a regional) assessment of metabolic wellbeing.

Points 1–3 can be summarised as: the CO is “x” l/min, which is adequate/inadequate for this patient at this time. Integration of CO into a global metabolic assessment necessitates an appreciation of the contribution of CO to oxygen delivery, and an understanding of the balance between oxygen delivery and consumption (table 1, fig 1). From a clinical perspective, this requires the consideration of four questions:

1. Is the delivery of oxygen adequate to meet the metabolic need of the patient, both on a global and a regional scale?
2. Is oxygen delivery occurring with an adequate perfusion pressure?
3. Is the delivery of oxygen adequate to meet the metabolic need of the patient, both on a global and a regional scale?
4. Is oxygen delivery occurring with an adequate perfusion pressure?
Is the patient able to utilise the oxygen delivered?

If the answer to any of the above is “no”, why is this so?

ADEQUACY OF CO AND OXYGEN DELIVERY
A variety of clinical, laboratory, and physiological variables exist which may help to indicate adequacy of CO and/or oxygen delivery.

Global indicators
Lactate
With the advent of automated blood lactate analysers, interest in this parameter has seen an explosion in the last decade. Simplistically, an increased blood lactate is thought to represent anaerobic metabolism, which occurs when oxygen delivery is inadequate, or oxygen utilisation is impaired (tissue dysoxia). Recent evidence suggests that this may be an oversimplification, as other factors such as increased glycolytic flux and lactate clearance may also play a part. Nonetheless this parameter has prognostic value, particularly when followed temporally, thus any increase in blood lactate is a cause for concern and the aetiology must be aggressively sought.

Mixed venous oxygen saturation
From the Fick principle (table 1) it can be seen that a low CO or excessive oxygen consumption can be partially compensated by an increase in the arteriovenous oxygen difference. This commonly translates into a fall in mixed venous saturation, as arterial blood is often almost fully saturated and the contribution of dissolved oxygen to total oxygen content is usually minimal. This is an early compensatory mechanism, and may precede a rise in blood lactate. Again, from the Fick equation, it can be seen that, at a constant oxygen consumption and arterial oxygen saturation, the relation between change in mixed venous saturation and CO is not linear, in other words a given decrease in mixed venous saturation may represent a comparatively larger decrease in CO (fig 2).

Mixed venous blood should ideally be taken from the pulmonary artery or the right ventricle; however, these sites may be inaccessible in the small infant. Right atrial catheters may, in theory selectively sample desaturated coronary venous blood; however, in practice this does not seem to be the case. Central venous sites have been advocated, although this is subject to ongoing debate. The oxygen saturation of central venous blood from either the superior or inferior vena cavae

Figure 1 Factors affecting oxygen delivery and consumption. BP, systemic blood pressure; SVR, systemic vascular resistance; VO2, oxygen consumption; A-V, atrioventricular; LVES, left ventricular end systolic. *Common intensive care scenarios augmenting intrathoracic pressure include mechanical ventilation, pneumothorax, pleural/pericardial fluid collections.

Figure 2 Relative change in cardiac index versus change in mixed venous oxygen saturation. The relation assumes the following to be constant: oxygen consumption 180 ml/min/m2, haemoglobin concentration 120 g/l, arterial oxygen saturation 98%. Baseline cardiac index is 4 l/min/m2.
will not be identical to true mixed venous blood, because of age and disease related variations in flow and oxygen consumption between the upper and lower body. However the differences may not be great, and may be suitable for trend following. Venous oxygen saturation will also be partly dependent on arterial oxygen saturation, thus the arteriovenous difference or the oxygen extraction ratio are better alternatives in the face of lung pathology (table 1). The inverse of the oxygen extraction ratio is known as the oxygen excess factor, or omega. Omega represents the ratio of oxygen delivery to consumption, and has an advantage over CO in that it may be calculated in the setting of an anatomical shunt.

Regional indicators
An apparently adequate global oxygen delivery may mask significant regional abnormalities. Unfortunately, comprehensive clinical tools assessing all aspects of regional perfusion are lacking; however, several of the common methods are detailed below.

Capillary refill and core-peripheral temperature difference
Provided that it is measured correctly, capillary refill has proven useful as a marker of hypovolaemia and perhaps poor myocardial function during acute assessment and early resuscitation. The significance of this parameter in ICU is less clear, and may be obscured by confounding factors such as fever, ambient temperature, and vasoactive medication use. Capillary refill correlates negatively with stroke volume, and the optimal predictive value for a reduced stroke volume comes from a refill time ≥6 seconds. There is no correlation with systemic vascular resistance. Despite these limitations, we believe capillary refill has a useful role in temporal haemodynamic monitoring. It is a quick, easy bedside test, and a dramatic change in this parameter should alert the clinician to a more detailed haemodynamic assessment of the patient. The correlation between core-peripheral temperature difference and invasive haemodynamic parameters is very poor; this parameter offers no real advantage over capillary refill.

Other regional indicators
A change in the level of consciousness in a patient with septic shock may be erroneously interpreted as secondary to “meningitis” or cerebral oedema; in reality this often represents cerebral hypoxia caused by lack of blood flow, and is, in our experience an ominous sign. Splanchnic oxygen delivery has been quantified using gastric tonometry. Here a semipermeable balloon is placed in the stomach, and gastric mucosal CO₂ is allowed to equilibrate with the medium in the balloon. The medium may be either saline or recirculating gas, the latter method being the more accurate. Regional hypoperfusion or failure of oxygen utilisation are revealed by a large difference between mucosal pCO₂, and arterial blood pCO₂. Ileus may be a clinical manifestation of splanchnic hypoperfusion; however, other causes must always be excluded. Similarly, one of the causes of acute derangement of liver transaminases may be inadequate hepatic oxygen delivery, and lack of renal blood flow may result in poor urine output and a rise in the serum urea and creatinine.

PERFUSION PRESSURE
Global perfusion pressure is measured via invasive arterial blood pressure monitoring. However, without CO measurement two erroneous inferences are possible: first, that an “adequate” blood pressure signifies an “adequate” CO; and second that manoeuvres that raise the blood pressure also result in elevation of CO (equation 1). In fact neither may be the case. The failing myocardium responds poorly to a high systemic vascular resistance; thus an increase in blood pressure may result in a fall in CO; conversely lowering the systemic vascular resistance with vasodilator therapy may produce a considerable gain in terms of CO despite a small drop in blood pressure.

OXYGEN CONSUMPTION
Oxygen consumption can now be measured at the bedside, even in the smallest patients, the commonest ICU method being indirect calorimetry. Providing that oxygen delivery and perfusion pressure are adequate, an inability to consume oxygen may be inferred without direct measurement from the combination of a raised blood lactate with a high mixed venous oxygen saturation.

IDENTIFYING THE SOURCE OF INADEQUATE OXYGEN DELIVERY OR EXCESSIVE CONSUMPTION
Oxygen delivery
Two of the components of oxygen delivery, haemoglobin concentration and arterial haemoglobin oxygen saturation, can be easily determined (table 1). The cause of a deficiency in the third component, CO is not always apparent, as this can be caused by abnormalities in heart rate, preload, contractility, afterload, or any combination of the four.

Heart rate
Heart rate is the easiest parameter to measure at the bedside. Cardiac output can be adversely affected by extreme sinus tachycardia (for example, with hypovolaemia or excessive inotrope use), bradycardia, or any arrhythmia producing loss of atrioventricular synchrony.

Preload
Preload encompasses the variety of factors resulting in ventricular end diastolic volume. It is important to appreciate that the preload of the right and left heart are not necessarily the same. The two commonly used measures of preload, namely central venous pressure (right heart) and pulmonary artery occlusion pressure (left heart) both have clinical limitations. This is because many factors affect the ability of a pressure measurement to act as a marker of volume status, including venous capacitance, cardiac chamber compliance, valve competence, pulmonary artery pressures, and the ability of the lung to function as a Starling resistor with positive pressure ventilation, to name a few. However it is probably reasonable to assume that a low central venous pressure may represent underfilling, and this parameter may be useful for trending.

Two new volume based measures, intrathoracic blood volume and right ventricular end diastolic volume, have been evaluated favourably as preload indicators. Both are calculated from modifications of a thermodilution technique; however, neither has been adequately evaluated in children. Analysis of variation in arterial pulse pressure waveform shows great promise, and can easily be incorporated into routine invasive blood pressure monitoring on a continuous basis. Several transoesophageal Doppler derived parameters have been explored; one has been used successfully in adults to guide intraoperative volume replacement. Two echocardiographic indicators of preload have been suggested. The functional preload index requires specialised software and a series of calculations, thus limiting its clinical use, while interpretation of mitral inflow velocity profiles is often beset by confounding variables. Diastolic dysfunction also affects preload, although controversy exists regarding the interpretation of echocardiographic parameters of diastolic function in certain clinical scenarios.
Contractility
An adequate bedside measure of contractility does not exist. The echocardiographic stress velocity index has provided insight into pathophysiology, but requires the same technical specifications as the functional preload index. Recently one of the assumptions on which this parameter is based, namely the linear relation between stress velocity (contractility) and end systolic wall stress (afterload) has been questioned, suggesting a reappraisal of its clinical interpretation.\(^7\) Stroke work index represents the area enclosed by the ventricular pressure-volume loop; however, this may be estimated at the bedside from stroke index and arterial pressure measurements (table 1). Although not a true measure of contractility, it allows some insight into cardiac reserve, namely how stroke index (volume) is adjusted in the face of changing afterload.

Afterload
Afterload is defined as the force opposing left ventricular fibre shortening during ventricular ejection, in other words left ventricular wall stress. Wall stress can be measured at various times throughout cardiac ejection, although it is thought that calculation at end systole provides the best measure of afterload.\(^8\) Calculation of wall stress requires measurement of end systolic transmural ventricular pressure, and echocardiographic measurement of left ventricular end systolic dimension and wall thickness.\(^9\) Here transmural pressure equals the difference between intra- and extraventricular (or intrathoracic) pressures. While intraventricular pressure can be estimated from the mean arterial pressure,\(^10\) accurate estimation of extraventricular/intrathoracic pressure is difficult and may involve measurement of oesophageal or pleural pressures. Using this approach it is easy to understand how factors that increase intrathoracic pressure, such as positive pressure ventilation, result in a reduction in afterload. A recent publication has suggested that the clinical contribution of extracardiac pressure when calculating indices of systolic function may in fact be minimal;\(^11\) however, whether this is so for calculation of afterload remains to be seen.

The commonest clinical measure of afterload is systemic vascular resistance. This parameter is analogous to Ohm’s law, treating the heart as a “DC” (constant) rather than an “AC” (pulsatile) generator of flow, by measuring the ratio of mean pressure drop across the systemic vascular bed to the flow (table 1). Seen in this light, the limitations of this calculation are obvious; however, it provides the clinician with a single figure that has prognostic value.\(^12\)

The importance of minimising afterload in the failing myocardium is well documented. However, the clinical dilemma is usually one of balancing afterload reduction against maintaining perfusion pressure (blood pressure); in reality this can only be optimised if CO is measured.

Oxygen consumption
Many clinical situations are known to elevate oxygen consumption (fig 1). Thus where an obvious oxygen supply:demand imbalance exists, reduction in oxygen consumption may be more fruitful than attempting to elevate delivery to supranormal levels.\(^13\) Examples include maintenance of normo- or mild hypothermia following cardiac surgery, provision of adequate analgesia and sedation, initiation of mechanical ventilation to decrease work of breathing, and avoidance of excessive doses of inotropic agents, thereby minimising potential for excessive thermogenesis and myocardial oxygen consumption.

SUMMARY
Systolic cardiac function comprises four interrelated variables: heart rate, preload, contractility, and afterload, which along with diastolic cardiac properties, result in CO. Accurate analysis of the components of cardiac function at the bedside is difficult, however measurement of CO in paediatric practice is now feasible. Interpretation of this parameter requires both a quantitative and a qualitative approach, which in turn requires the integration of a wide array of physiological, laboratory, and clinical parameters. Understanding cardiovascular output should always be considered in terms of its contribution to global oxygen delivery/consumption balance.

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