Lung Mechanics in Normal Infants and Infants with Congenital Heart Disease

GERALDINE HOWLETT

From the Department of Paediatrics, Institute of Diseases of the Chest, London

Howlett, G. (1972). Archives of Disease in Childhood, 47, 707. Lung mechanics in normal infants and infants with congenital heart disease. The results of a study of pulmonary mechanics in 24 normal infants and 28 infants with congenital heart disease aged 1 to 32 weeks are presented. The two groups were matched for length and weight. The diagnosis of the infants with congenital heart disease varied from simple stenoses to complex septal defects and transpositions. 6 infants were studied before and after operation designed to improve their haemodynamic situation.

Pulmonary compliance and mean pulmonary resistance were measured using a pneumotachygraph, integrator, and oesophageal balloon; thoracic gas volume was measured by the plethysmographic method. Results were found to be reproducible both in the individual and within the normal group.

Thoracic gas volume in relation to weight and pulmonary resistance were normal in the infants with congenital heart disease, but the pulmonary compliance was often abnormal even when related to lung volume. The change in compliance was not simply related to pulmonary blood flow or pressure but was related to the radiological assessment of pulmonary plethora or oligaemia—the more plethora the lower the compliance. Surgery altered both the radiological grading and the compliance appropriately. It is postulated that changes in the elastic properties of the lungs are related to changes in the pulmonary capillary blood volume.

The alteration in pulmonary haemodynamics due to various congenital cardiac malformations has been shown in previous studies on adults (Saxton et al., 1956; Davies, Williams, and Wood, 1962; Davies and Gazetopoulos, 1967), children (Wallgren, Geubelle, and Koch, 1960; Ohnishi, 1970), and experimental animals (Borst et al., 1957; Cook et al., 1959) to have an effect upon the mechanical behaviour of the lungs. The present study was undertaken to investigate this effect in neonates and infants with congenital heart disease in order to see whether measurements of lung mechanics could be used to assess the severity of the cardiac defect and to evaluate the effect of surgery.

Normal values of lung volume and mechanical behaviour are available for infants in the first week or two of life (Klaus et al., 1962; Auld et al., 1963; Cook et al., 1957; Swyer, Reiman, and Wright, 1960) but there are only a few reports of measurements made on infants beyond this age (Wallgren et al., 1960; Krieger, 1963; Phelan and Williams, 1969; Doershuk et al., 1970). Because there is a wide scatter in the normal results quoted by these workers the various parameters of lung function were also measured in a comparable group of normal infants to serve as controls.

Subjects

Normal infants. 24 normal infants were studied between the ages of 1 week and 8 weeks, 2 infants being studied twice. There was no history of any pulmonary or other complication at birth or in the postnatal period, and on the day of the study all infants were clinically normal. Eight infants were studied at the age of 1 week on the day before discharge and the others were studied at a later date when their mothers brought them back to the laboratory. Written permission was obtained from the mother in all cases, after a full explanation of the procedures involved.

Infants with congenital heart disease. 28 infants with congenital heart disease were studied and of these 21 had cardiac catheter studies within 1 to 2 weeks of

Received 30 March 1972.
the lung function tests, there having been no alteration in treatment between the two investigations. 6 infants were also studied before and after operations undertaken to decrease right-to-left shunting in 1 infant by relieving a pulmonary stenosis, and to decrease a left-to-right shunt in 5 others. The diagnosis varied from a simple persistent ductus arteriosus to complicated septal defects and transposition of the great arteries, and therefore could not be placed in simple groups. The details of the diagnosis and the various parameters of pulmonary haemodynamics in those infants who were catheterized are given in Table I.

### Methods and Calculations

The method used in this study was similar to that described by Phelan and Williams (1969). The infant was lightly sedated with chloral hydrate 60 mg/kg fairly soon after a feed. A small latex balloon, 5·0 cm long, 1·8 cm in circumference, and containing approximately 0·2 ml of air, was passed via the mouth to the middle-third of the oesophagus. Respiratory changes in oesophageal pressure were recorded by an S.E. Laboratories 1150/D5964 pressure transducer. The infant was then placed in a body plethysmograph of the same design as that described by Cross (1949). Siliconized putty was used to seal the plethysmograph around the nose and mouth as described by Burnard et al. (1965). Airflow was recorded at the mouth by means of a mercury electronics pneumotachograph (resistance 1·4 cmH₂O/l/sec) and a Sierex E.M.T. 32 pressure transducer, and the output was electrically integrated to give tidal volume.

During a period of quiet breathing the above parameters were recorded on an Ampex Electromagnetic Tape Recorder (SP 300). When all the measurements had been made the tape was replayed through a Lan-Electronics 419B oscilloscope, and 10 consecutive quiet breaths were selected for further analysis. The pressure-volume and flow-volume loops for each breath were plotted by means of a Bryans X-Y auto-plottter and examples of these loops for one breath are shown in Fig. 1.

From the pressure-volume loop pulmonary compliance (Cₚ) was calculated as the ratio between volume change and the corresponding oesophageal pressure change at points of no flow. Mean pulmonary resistance (Rₚ) was calculated as the ratio between total pressure change and total flow change between points of equal

---

**TABLE I**

Diagnosis, X-ray Grading of Pulmonary Vasculature, and Cardiac Catheterization Results in Infants with Congenital Heart Disease

<table>
<thead>
<tr>
<th>Case No.</th>
<th>Age (wk)</th>
<th>Mean Pulmonary Artery Pressure (mmHg)</th>
<th>Pulmonary Flow (l/min per m²)</th>
<th>X-ray Grading*</th>
<th>Diagnosis†</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>1½</td>
<td>27·5</td>
<td>28·0</td>
<td>3</td>
<td>VSD, PDA, ASD, coarctation</td>
</tr>
<tr>
<td>2</td>
<td>12</td>
<td>30·0</td>
<td>7·3</td>
<td>2</td>
<td>PDA, VSD, coarctation</td>
</tr>
<tr>
<td>3</td>
<td>6</td>
<td>55·0</td>
<td>5·6</td>
<td>2</td>
<td>Truncus arteriosus</td>
</tr>
<tr>
<td>4</td>
<td>5</td>
<td>—</td>
<td>4·7</td>
<td>2</td>
<td>TGA, VSD, PDA, coarctation</td>
</tr>
<tr>
<td>5</td>
<td>2</td>
<td>—</td>
<td>1·4</td>
<td>3</td>
<td>PS, ASD</td>
</tr>
<tr>
<td>6</td>
<td>8</td>
<td>9·0</td>
<td>—</td>
<td>1</td>
<td>PDA, pulmonary hypertension</td>
</tr>
<tr>
<td>7</td>
<td>18</td>
<td>55·0</td>
<td>2·9</td>
<td>—1</td>
<td>Tricuspid atresia, VSD</td>
</tr>
<tr>
<td>8</td>
<td>2</td>
<td>—</td>
<td>3·4</td>
<td>0</td>
<td>VSD, ASD, PS, anomalous venous return</td>
</tr>
<tr>
<td>9</td>
<td>3</td>
<td>18·0</td>
<td>11·6</td>
<td>3</td>
<td>TGA, VSD, PDA</td>
</tr>
<tr>
<td>10</td>
<td>7</td>
<td>38·5</td>
<td>—</td>
<td>1</td>
<td>MI, coarctation, common ventricle</td>
</tr>
<tr>
<td>11</td>
<td>10</td>
<td>39·0</td>
<td>4·2</td>
<td>2</td>
<td>Atrioventricular canal</td>
</tr>
<tr>
<td>12</td>
<td>32</td>
<td>42·0</td>
<td>9·3</td>
<td>1</td>
<td>VSD, PS</td>
</tr>
<tr>
<td>13</td>
<td>17</td>
<td>32·5</td>
<td>17·5</td>
<td>2</td>
<td>VSD</td>
</tr>
<tr>
<td>14</td>
<td>17</td>
<td>35·0</td>
<td>11·6</td>
<td>1</td>
<td>Mitral atresia, VSD, ASD</td>
</tr>
<tr>
<td>15</td>
<td>1</td>
<td>—</td>
<td>7·4</td>
<td>0</td>
<td>Cardiomegaly</td>
</tr>
<tr>
<td>16</td>
<td>24</td>
<td>20·0</td>
<td>3·0</td>
<td>1</td>
<td>VSD, PDS, coarctation</td>
</tr>
<tr>
<td>17</td>
<td>11</td>
<td>76·0</td>
<td>4·0</td>
<td>3</td>
<td>TGA, ASD, VSD, coarctation</td>
</tr>
<tr>
<td>18</td>
<td>1</td>
<td>43·0</td>
<td>2·5</td>
<td>0</td>
<td>PDA, VSD</td>
</tr>
<tr>
<td>19</td>
<td>14</td>
<td>42·0</td>
<td>11·7</td>
<td>0</td>
<td>VSD, ASD</td>
</tr>
<tr>
<td>20</td>
<td>5</td>
<td>10·0</td>
<td>1·4</td>
<td>1</td>
<td>PS, VSD</td>
</tr>
<tr>
<td>21</td>
<td>7</td>
<td>57·0</td>
<td>4·1</td>
<td>1</td>
<td>PDA, VSD, coarctation</td>
</tr>
<tr>
<td>22</td>
<td>6</td>
<td>—</td>
<td>10·8</td>
<td>3</td>
<td>VSD, PDA</td>
</tr>
<tr>
<td>23</td>
<td>12</td>
<td>—</td>
<td>—</td>
<td>0</td>
<td>TGA, PDA, ASD, PDA</td>
</tr>
<tr>
<td>24</td>
<td>1½</td>
<td>—</td>
<td>—</td>
<td>0</td>
<td>VSD, ASD</td>
</tr>
<tr>
<td>25</td>
<td>3</td>
<td>—</td>
<td>—</td>
<td>0</td>
<td>Truncus arteriosus, VSD</td>
</tr>
<tr>
<td>26</td>
<td>1</td>
<td>—</td>
<td>—</td>
<td>0</td>
<td>TGA, VSD, ASD</td>
</tr>
<tr>
<td>27</td>
<td>2</td>
<td>—</td>
<td>—</td>
<td>1</td>
<td>VSD, PDA</td>
</tr>
<tr>
<td>28</td>
<td>4</td>
<td>—</td>
<td>—</td>
<td>0</td>
<td>VSD, PS</td>
</tr>
</tbody>
</table>

*—1, oligemic; 0, normal; 1, 2, and 3, increasing plethora. PDA, persistent ductus arteriosus; VSD, ventricular septal defect; PS pulmonary stenosis; ASD, atrial septal defect; TGA, transposition of great arteries; MI, mitral incompetence.

Note: In those infants for whom catheter data are not given, either the pulmonary artery was not entered or the diagnosis was made on clinical grounds or at necropsy.
Lung Mechanics in Normal Infants and Infants with Congenital Heart Disease

Fig. 1.—Pressure-volume and flow-volume loops plotted from a single breath. \( V_T \) = tidal volume, \( \Delta P_{EL} \) = change in oesophageal pressure between points of zero flow, \( \Delta P_I \) and \( \Delta P_E \) = pressure required to overcome resistive forces at midinspiratory and midexpiratory volumes, respectively, \( \Delta V_I \) and \( \Delta V_E \) = flow rates at midinspiratory and midexpiratory volume, respectively.

Volume midway in inspiration and expiration (see Fig. 1).

The reproducibility of these 10 measurements in each individual was such that the mean coefficients of variation (SD/mean) in the normal infants were 5.7% for \( C_L \) and 7.9% for \( R_L \), respectively, and in the cardiac infants they were 8.9% and 10.1%, respectively.

Thoracic gas volume (TGV) was measured by a plethysmographic technique. Airflow was interrupted at the mouth by suddenly inflating a balloon which was lying in the lumen of the pneumotachograph. As the infant continued to make respiratory efforts, mouth pressure and plethysmograph pressure changes were recorded on the tape recorder by means of S.E. Laboratories 1150/D5964 pressure transducers. TGV was then calculated by the method of Dubois et al. (1956) and corrected to end-expiratory level, and was therefore identical with functional residual capacity (FRC). This procedure was repeated 4 times and the mean result calculated.

The chest x-rays of the infants with congenital heart disease were examined by an experienced radiologist with regard to their pulmonary vasculature. They were presented to him on two separate occasions, in random order, without his knowledge of the physiological results or the fact that he was seeing the same films twice. The pulmonary vasculature was graded as being normal, oligemic, or plethoric 1—3, and the results of the grading for the individual infants are also shown in Table I.

Results

Normal infants. The relations between TGV and body weight, and between \( C_L \) and TGV were both highly significant \( (P < 0.001) \) and are illustrated in Fig. 2 and 3. Not only was the \( C_L \)-TGV relation linear but the regression line also passed through zero. The ratio of compliance to TGV, Fig. 2.—Relation between thoracic gas volume and body weight for normal infants. The calculated regression line for this and subsequent figures is shown together with \( \pm 1 \) standard error of the estimate of \( y \) about the line. The regression equation is \( y = 32.47 x + 11.61 \) \( (r = 0.955; P < 0.001) \).
Fig. 3.—Relation between compliance and thoracic gas volume for normal infants. The regression equation is 
\[ y = 0.0597x + 0.372 \ (r = 0.89; \ P < 0.001). \]

Specific compliance (SCV), was therefore constant and could be used to compare different individuals.

The coefficients of variation for the normal group of TGV/kg and specific compliance were 5.1% and 7.3%, respectively, indicating that when TGV and compliance were corrected for body size there was only a narrow scatter in the normal results.

When conductance, the reciprocal of resistance, was related to TGV the relation was not significant (\( P = 0.1 \)) in these infants. However, the range of values was small, the mean and 1 SD being 20.6 ± 3.8 (cmH₂O/l. per sec) for resistance.

**Infants with congenital heart disease.** The pulmonary function data from the individual infants with congenital heart disease are shown in Table II and the mean values are compared with those from the normal children in Table III.

The mean weight (3.55 kg) and length (53.3 cm) were slightly below those for the normal infants. The mean frequency of breathing (72 ± 15.2 breaths/min) was increased, that of the normal infants being 58.4 ± 12.6 breaths/min. There was no significant difference between the tidal volume/kg or the \( R_L \) compared to the normal infants. The mean TGV for the cardiac infants was not significantly different from the normal infants when corrected for differences in body weight (Fig. 4).

When \( C_L \) was related to TGV the individual results often differed significantly from the normal (Fig. 5). The value given in Table III as the

### TABLE II

**Pulmonary Function Data From Infants with Congenital Heart Disease**

<table>
<thead>
<tr>
<th>Case No.</th>
<th>Weight (kg)</th>
<th>Length (cm)</th>
<th>Frequency (breaths/min)</th>
<th>Tidal Volume (ml)</th>
<th>TGV (ml)</th>
<th>( C_L ) (ml/cmH₂O)</th>
<th>( R_L ) (cmH₂O/l. per sec)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>3.08</td>
<td>48.5</td>
<td>56</td>
<td>18.2</td>
<td>95.6</td>
<td>2.39</td>
<td>27.70</td>
</tr>
<tr>
<td>2</td>
<td>4.05</td>
<td>61.0</td>
<td>60</td>
<td>42.3</td>
<td>180.7</td>
<td>5.20</td>
<td>35.50</td>
</tr>
<tr>
<td>3</td>
<td>3.57</td>
<td>55.0</td>
<td>60</td>
<td>37.1</td>
<td>130.0</td>
<td>5.77</td>
<td>17.38</td>
</tr>
<tr>
<td>4</td>
<td>3.04</td>
<td>49.0</td>
<td>20.8</td>
<td>22.8</td>
<td>99.0</td>
<td>3.52</td>
<td>30.30</td>
</tr>
<tr>
<td>5</td>
<td>3.25</td>
<td>54.0</td>
<td>85</td>
<td>30.5</td>
<td>117.0</td>
<td>3.80</td>
<td>22.70</td>
</tr>
<tr>
<td>6</td>
<td>4.44</td>
<td>54.5</td>
<td>45</td>
<td>64.3</td>
<td>147.6</td>
<td>13.25</td>
<td>18.50</td>
</tr>
<tr>
<td>7</td>
<td>3.98</td>
<td>50.5</td>
<td>80</td>
<td>56.0</td>
<td>136.0</td>
<td>10.89</td>
<td>14.95</td>
</tr>
<tr>
<td>8</td>
<td>2.24</td>
<td>44.0</td>
<td>67</td>
<td>35.8</td>
<td>79.0</td>
<td>9.68</td>
<td>18.20</td>
</tr>
<tr>
<td>9</td>
<td>3.58</td>
<td>52.0</td>
<td>85</td>
<td>32.8</td>
<td></td>
<td>4.52</td>
<td>24.60</td>
</tr>
<tr>
<td>10</td>
<td>3.04</td>
<td>56.0</td>
<td>100</td>
<td>30.9</td>
<td></td>
<td>7.36</td>
<td>21.10</td>
</tr>
<tr>
<td>11</td>
<td>11.75</td>
<td>54.0</td>
<td>65</td>
<td>32.5</td>
<td></td>
<td>5.94</td>
<td>29.60</td>
</tr>
<tr>
<td>12</td>
<td>4.28</td>
<td>61.0</td>
<td>75</td>
<td>52.6</td>
<td>163.0</td>
<td>8.53</td>
<td>20.80</td>
</tr>
<tr>
<td>13</td>
<td>3.93</td>
<td>54.0</td>
<td>57</td>
<td>47.6</td>
<td>160.2</td>
<td>7.72</td>
<td>31.00</td>
</tr>
<tr>
<td>14</td>
<td>5.04</td>
<td>61.0</td>
<td>82</td>
<td>41.6</td>
<td>163.5</td>
<td>9.90</td>
<td>15.00</td>
</tr>
<tr>
<td>15</td>
<td>3.04</td>
<td>48.0</td>
<td>75</td>
<td>35.0</td>
<td>118.0</td>
<td>7.14</td>
<td>21.00</td>
</tr>
<tr>
<td>16</td>
<td>5.40</td>
<td>68.5</td>
<td>95</td>
<td>39.0</td>
<td>166.5</td>
<td>5.42</td>
<td>13.10</td>
</tr>
<tr>
<td>17</td>
<td>3.44</td>
<td>53.0</td>
<td>85</td>
<td>31.8</td>
<td>135.2</td>
<td>5.85</td>
<td>37.50</td>
</tr>
<tr>
<td>18</td>
<td>3.15</td>
<td>48.0</td>
<td>80</td>
<td>29.6</td>
<td>92.5</td>
<td>4.90</td>
<td>21.10</td>
</tr>
<tr>
<td>19</td>
<td>2.47</td>
<td>50.0</td>
<td>80</td>
<td>25.2</td>
<td></td>
<td>5.58</td>
<td>18.80</td>
</tr>
<tr>
<td>20</td>
<td>4.09</td>
<td>54.0</td>
<td>42</td>
<td>61.0</td>
<td>135.5</td>
<td>10.81</td>
<td>27.00</td>
</tr>
<tr>
<td>21</td>
<td>2.30</td>
<td>48.0</td>
<td>80</td>
<td>26.6</td>
<td>75.8</td>
<td>3.50</td>
<td>25.50</td>
</tr>
<tr>
<td>22</td>
<td>3.50</td>
<td>50.0</td>
<td>20.2</td>
<td>22.8</td>
<td></td>
<td>2.08</td>
<td>43.50</td>
</tr>
<tr>
<td>23</td>
<td>4.38</td>
<td>57.0</td>
<td>70</td>
<td>35.0</td>
<td>150.0</td>
<td>9.33</td>
<td>17.75</td>
</tr>
<tr>
<td>24</td>
<td>3.02</td>
<td>48.0</td>
<td>68</td>
<td>33.5</td>
<td>93.4</td>
<td>5.07</td>
<td>22.40</td>
</tr>
<tr>
<td>25</td>
<td>2.04</td>
<td>46.0</td>
<td>96</td>
<td>18.6</td>
<td>71.0</td>
<td>2.26</td>
<td>35.60</td>
</tr>
<tr>
<td>26</td>
<td>3.66</td>
<td>53.0</td>
<td>60</td>
<td>38.1</td>
<td>133.5</td>
<td>8.08</td>
<td>17.20</td>
</tr>
<tr>
<td>27</td>
<td>2.98</td>
<td>52.0</td>
<td>94</td>
<td>28.0</td>
<td>110.0</td>
<td>5.07</td>
<td>33.80</td>
</tr>
<tr>
<td>28</td>
<td>3.37</td>
<td>53.0</td>
<td>60</td>
<td>31.0</td>
<td>115.0</td>
<td>5.07</td>
<td>40.60</td>
</tr>
</tbody>
</table>

*Note:* TGV, thoracic gas volume; \( C_L \), pulmonary compliances; \( R_L \), mean pulmonary resistance.
Lung Mechanics in Normal Infants and Infants with Congenital Heart Disease

TABLE III
Mean Pulmonary Function Data from Normal Infants and Infants with Congenital Heart Disease

<table>
<thead>
<tr>
<th>Measurement</th>
<th>Normal</th>
<th>Cardiac</th>
<th>Significance of Difference Between Means</th>
</tr>
</thead>
<tbody>
<tr>
<td>Weight (kg)</td>
<td>4·01±0·66</td>
<td>3·55±0·82</td>
<td>P &lt; 0·001</td>
</tr>
<tr>
<td>Length (cm)</td>
<td>55·8±2·97</td>
<td>53·3±5·4</td>
<td>P = 0·05</td>
</tr>
<tr>
<td>Frequency (breaths/min)</td>
<td>58·4±12·6</td>
<td>72·0±15·2</td>
<td>P &lt; 0·001</td>
</tr>
<tr>
<td>Tidal volume/kg (ml)</td>
<td>10·39±1·27</td>
<td>9·61±2·18</td>
<td>NS</td>
</tr>
<tr>
<td>Thoracic gas volume/kg (ml)</td>
<td>35·5±1·78</td>
<td>34·4±3·16</td>
<td>NS</td>
</tr>
<tr>
<td>Specific compliance (ml/cmH2O per ml TGV)</td>
<td>0·062±0·0045</td>
<td>0·047±0·015</td>
<td>P &lt; 0·001</td>
</tr>
<tr>
<td>Mean pulmonary resistance (cmH2O/l per sec)</td>
<td>20·57±3·8</td>
<td>23·95±7·42</td>
<td>NS</td>
</tr>
</tbody>
</table>

NS, not significant.

The mean SCL for the cardiac infants (0·047 ml/cmH2O per ml TGV) was the mean of those infants with left-to-right shunts and as a group they differ significantly from normal (P < 0·001). All the infants with an increase in both pulmonary artery pressure and flow had a reduction in SCL while in those infants with increased pulmonary pressure or flow alone the difference from normal was not so significant. The two infants with a decrease in both pulmonary pressure and flow had an increased SCL.

![Fig. 4](http://adc.bmj.com/)

**FIG. 4.—Relation between thoracic gas volume and weight for infants with congenital heart disease is shown superimposed on the regression line for normal infants.**

![Fig. 5](http://adc.bmj.com/)

**FIG. 5.—Relation between compliance and thoracic gas volume for infants with congenital heart disease is shown superimposed on the regression line for normal infants.**

P = mean pulmonary artery pressure, F = pulmonary flow.

When the SCL of the infants with congenital heart disease was related to mean pulmonary artery pressure or to pulmonary flow (Fig. 6a and 6b), no definite relation was found. But, when related to the product of pulmonary artery pressure and flow (the 'hyperkinetic index', Davies and Gazetopoulus, 1967) the relation was moderately significant (P < 0·02—Fig. 6c).

There was a very close relation between SCL and the radiological grading of pulmonary plethora such that as the degree of plethora increased so the compliance of the lungs decreased (Fig. 7). Moreover, in the 6 infants who were studied before and after operation, as the radiological grading altered so did the compliance (Fig. 8). Cases 1 to 5 all had operations to reduce a left-to-right shunt and
Fig. 6a, b, and c.—Specific compliance related (a) to mean pulmonary artery pressure, (b) to pulmonary flow and (c) to the product of pressure and flow (the hyperkinetic index), in infants with congenital heart disease. Horizontal lines represent the normal mean specific compliance (± 2 SD). Solid vertical lines in (a) and (b) represent the mean normal pressure and flow, respectively.

Fig. 7.—Specific compliance related to the radiological grading of pulmonary plethora. Solid line represents the mean normal specific compliance (± 2 SD).

Fig. 8.—Change in the relation between specific compliance and radiological grading of pulmonary plethora in the 6 infants with congenital heart disease who were studied both before and after operation. The early postoperative study was done on the 5th and 6th day, and the late postoperative study was done between 4 to 6 weeks after the operation. Numbers 1 to 5 refer to children who had raised pulmonary flow initially, and number 6 refers to the child with reduced flow initially.
in the 4 infants on whom measurements were made 4 to 6 weeks postoperatively both the radiological grading and the compliance had returned to within normal limits. In the one infant, Case 6, who was studied before and after pulmonary valvotomy and reduction to right-to-left shunt, the compliance and radiological grading both improved. Thoracic gas volume was not significantly altered in these infants so that the changes in compliance were not due to volume.

**Discussion**

These results show that the compliance of the lungs often differs from normal in infants with congenital heart disease even when it is related to lung volume.

**Normal results.** The results obtained from the normal infants differ in some respects from those found in studies on younger infants (Cook et al., 1957; Swyer et al., 1960). The mean tidal volume and frequency were higher and the mean pulmonary resistance was lower but they are more similar to the results found in older infants (Phelan and Williams, 1969; Doershuk et al., 1970).

The larger tidal volume and respiratory rate noted in the present study was most likely due to the size of the dead space of the system which was approximately 20 ml. However, this method proved to be the simplest and most reproducible for the measurement of compliance and thoracic gas volume (corrected for the dead space) which were of primary interest to the present study.

The techniques used in the present study are identical with those used by Phelan and Williams (1969), and the similarity of the results suggests that differences in techniques are in fact among the main reasons for the wide scatter of normal results quoted in the literature. The very good reproducibility and narrow scatter both within the individual and the normal group results obtained in the present study indicate that this method could be used for comparisons between the infants with congenital heart disease and the normal control group.

The highly significant correlation between TGV and body weight (Fig. 2) is in agreement with many other workers, and the mean value 35.5 ml/kg is comparable with that quoted by Phelan and Williams (1969), 31.5 ml/kg, Doershuk et al. (1970), 32.4 ml/kg; and Auld et al. (1963) 35.8 ml/kg. Similarly, the significant relation between C_L and TGV (Fig. 3) has been found by other workers. The mean S_C_L of 0.062 ml/cmH_2O per ml TGV is a little higher than that quoted by Phelan and Williams (1969) of 0.056 ml/cmH_2O per ml TGV, but it is within the generally accepted range.

The fact that there was no significant relation between conductance and TGV was probably due to the relatively small size range of the infants studied because a good correlation was obtained by Doershuk et al. (1970) over a much larger range. However, the absolute value for pulmonary resistance (or conductance) was within the range found by other workers for infants (Swyer et al., 1960; Krieger, 1963).

**Infants with congenital heart disease.** The effect of altered pulmonary haemodynamics upon the mechanical behaviour of the lungs has been investigated by several workers since it was originally suggested by von Basch (1887) that vascular congestion in the lungs might cause a stiffening of the parenchyma, and by Eisenmenger (1898) that in ventricular septal defect the pulmonary circulation was overfilled and the lungs stiffer. However, virtually all the results quoted to date have been obtained from adults and older children (Saxton et al., 1956; Davies et al., 1962; Davies and Gazetopoulos, 1967). It has been possible to find only one reference (Wallgren et al., 1960) which quotes figures for infants, and of the 25 infants they studied only 9 were less than 6 months of age. It is therefore of some significance that the results obtained in the present study on neonates and infants, whose pulmonary mechanics and circulation are presumably more labile, are very similar to those quoted for older children and adults.

Wallgren et al. (1960) suggested that the reduction in compliance found in the presence of left-to-right shunt might be due to a reduction in the aerated lung volume. The findings of the present study that TGV was not reduced in infants with congenital heart disease is in agreement with Davies and Gazetopoulos (1967) who found that the measured FRC in 38 adult patients with various forms of left-to-right shunt did not differ significantly from the predicted FRC. Wallgren et al. (1960) did not measure lung volume during their study and the present findings tend to disprove their theory.

The good correlation between compliance and TGV (Fig. 3) enabled a comparison to be made between the normal infants and the cardiac infants. The reduced S_C_L in the infants with left-to-right shunts is in agreement with Wallgren et al. (1960), Davies et al. (1962), and Ohnishi (1970) in older subjects. The lack of significant correlation between specific compliance and pulmonary arterial pressure or flow in the present study confirms the previous findings in older subjects (Saxton et al.,...
1956; Davies et al., 1962; Davies and Gazetopoulos 1967; Wallgren et al., 1960). The explanation remains uncertain and could even be coincidental. It could be suggested that interstitial changes such as incipient or actual pulmonary oedema could have reduced the compliance but the fact that the $C_L$ was increased in the two cases with a reduction in pulmonary pressure and flow makes the hypothesis unlikely. Moreover, one would not expect the thoracic gas volume and pulmonary resistance to be normal in the face of major interstitial changes.

It has been suggested that an increase in the actual blood volume present in the pulmonary vessels may be the major factor in altering the mechanics of the lungs. Mills (1949) found that altering the pulmonary blood volume in adult subjects altered the vital capacity. Harada (1959) studied healthy adult dogs before and after lung resection and found a positive correlation between the postoperative changes in pulmonary blood volume and decrease in the effective pulmonary compliance.

Bondurant, Hickam, and Isley (1957) reported a rapid decrease in compliance after the induction of acute central venous congestion in normal human subjects. The findings of the present study that the radiological grading of the pulmonary vasculature correlated closely with $C_L$ suggests that the actual blood volume is an important factor in altering lung mechanics in heart disease. As the lungs became more plethoric so the specific compliance fell and vice versa. Moreover, the specific compliance and pulmonary vascularity changed in the appropriate direction as a result of surgery. Haughton (1968) studied 3 adults with pulmonary stenosis and found that the compliance was high before operation and fell strikingly after valvotomy.

In conclusion therefore, infants with congenital heart disease have normal lung volumes and resistance to air flow, but a disturbance of the elastic properties of their lungs. When the lungs are plethoric with high pulmonary artery pressure and increased blood flow they are stiffer than normal. When they are oligemic with low pulmonary artery pressure and reduced blood flow their elasticity is increased. The elastic properties can be changed acutely by surgery. It is postulated that the changes in elastic properties are related to changes in pulmonary capillary blood volume.

I thank Drs. A. P. Norman and D. R. Harvey for allowing me to study normal infants at Queen Charlotte’s Maternity Hospital, and Dr. G. Simons for his interpretation of the x-rays; also Dr. S. Godfrey for his help and advice; and Miss G. Earle and the staff of the Paediatric Unit at the Brompton Hospital for their assistance.

The author was in receipt of a grant from The Medical Research Council during the period of this study.

References


**Lung Mechanics in Normal Infants and Infants with Congenital Heart Disease**


**Addendum**

Since this work was completed, Griffin *et al.* (1972) have published their findings of similar studies in infants with congenital heart disease and have come to similar conclusions.

**Reference**


Correspondence to Dr. G. Howlett, Paediatric Department, Institute of Diseases of the Chest, Fulham Road, London SW3.
Lung Mechanics in Normal Infants and Infants with Congenital Heart Disease

Geraldine Howlett

Arch Dis Child 1972 47: 707-715
doi: 10.1136/adc.47.255.707

Updated information and services can be found at:
http://adc.bmj.com/content/47/255/707

Email alerting service

These include:
Receive free email alerts when new articles cite this article. Sign up in the box at the top right corner of the online article.

Notes

To request permissions go to:
http://group.bmj.com/group/rights-licensing/permissions

To order reprints go to:
http://journals.bmj.com/cgi/reprintform

To subscribe to BMJ go to:
http://group.bmj.com/subscribe/